



A Modular Platform for Cell Characterization, Handling and Sorting by Dielectrophoresis

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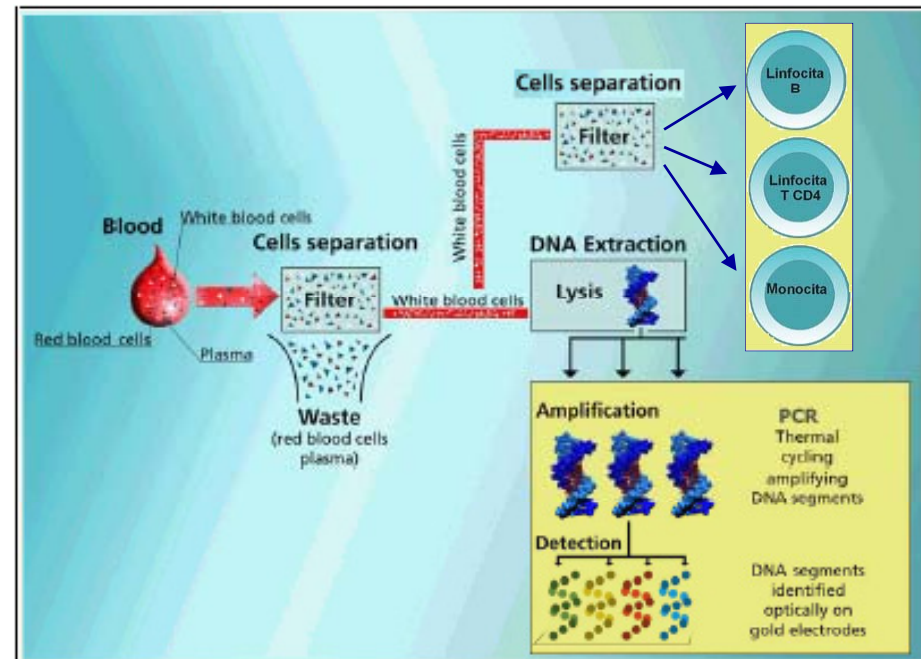


A mature product:

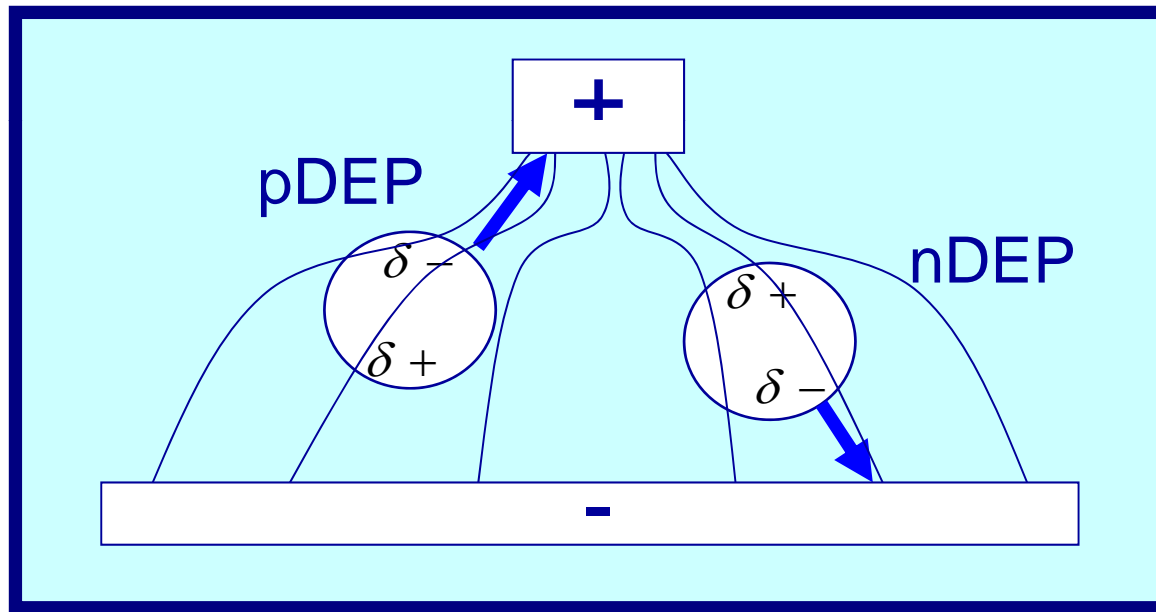
InCheck, a lab-on-chip for DNA amplification by Polymerase Chain Reaction (PCR) and analysis

Research:

on-chip solutions for cell analysis (microcytometry, cell sorting and cell counting applications)



Dielectrophoresis (DEP) is a promising method for cell manipulation and separation without physical contact, exploiting the dielectric properties of cells under the action of high-gradient electric fields.



$$\bar{F} = (\bar{m} \square \nabla) \bar{E}$$

$$\bar{m} = 4\pi\epsilon_m \textcircled{F_{CM}} R^3 \bar{E}$$

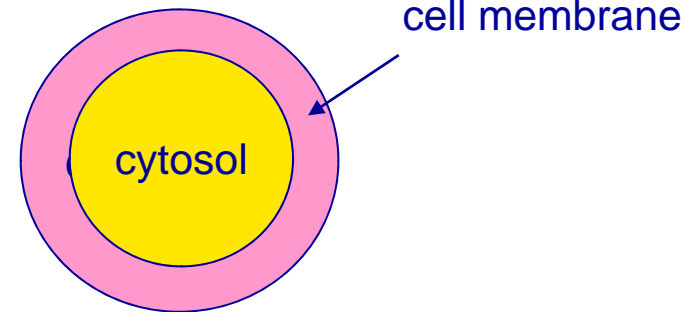
Clausius-Mosotti factor

$$F_{CM} = \frac{\epsilon_p^* - \epsilon_m^*}{\epsilon_p^* + 2\epsilon_m^*}$$

$$\epsilon_m^*(\omega) = \epsilon_m - \frac{j\sigma_m}{\omega}$$

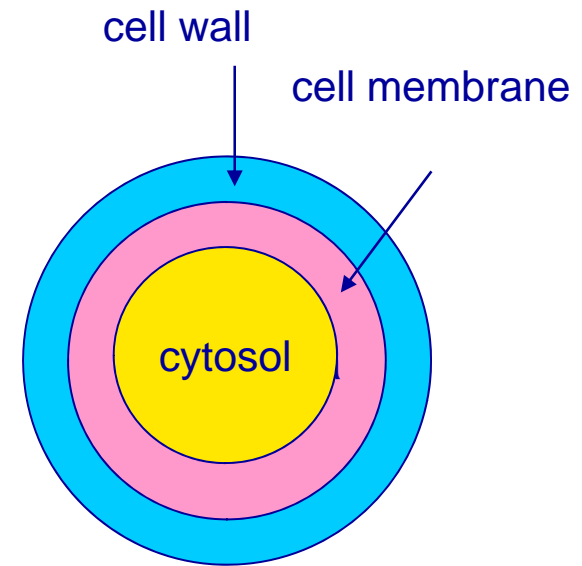
Suspending medium

$$\epsilon_p^* = \epsilon_{mc}^* \left[\frac{\left(\frac{r}{r-d}\right)^3 + 2\left(\frac{\epsilon_{int}^* - \epsilon_{mc}^*}{\epsilon_{int}^* + 2\epsilon_{mc}^*}\right)}{\left(\frac{r}{r-d}\right)^3 - \left(\frac{\epsilon_{int}^* - \epsilon_{mc}^*}{\epsilon_{int}^* + 2\epsilon_{mc}^*}\right)} \right]$$



*Cell with single membrane
(human B-lymphocytes)*

$$\mathbf{\rightarrow} \quad \epsilon_p^* = \epsilon_w^* \cdot \frac{2 \cdot \left(1 - \left(\frac{r - d_w}{r}\right)^3\right) \cdot \epsilon_w^* + \left(1 + 2 \cdot \left(\frac{r - d_w}{r}\right)^3\right) \cdot \epsilon_{\text{int}+mc}^*}{\left(2 + \left(\frac{r - d_w}{r}\right)^3\right) \cdot \epsilon_w^* + \left(1 - \left(\frac{r - d_w}{r}\right)^3\right) \cdot \epsilon_{\text{int}+mc}^*}$$



Cells with double shell model

(Saccharomyces Cerevisiae yeast cells with membrane and wall)

$$\epsilon_{\text{int}+mc}^* = \epsilon_{mc}^* \cdot \frac{2 \cdot \left(1 - \left(1 - \frac{d_{mc}}{r - d_w}\right)^3\right) \cdot \epsilon_{mc}^* + \left(1 + 2 \cdot \left(1 - \frac{d_{mc}}{r - d_w}\right)^3\right) \cdot \epsilon_{\text{int}}^*}{\left(2 + \left(1 - \frac{d_{mc}}{r - d_w}\right)^3\right) \cdot \epsilon_{mc}^* + \left(1 - \left(1 - \frac{d_{mc}}{r - d_w}\right)^3\right) \cdot \epsilon_{\text{int}}^*}$$

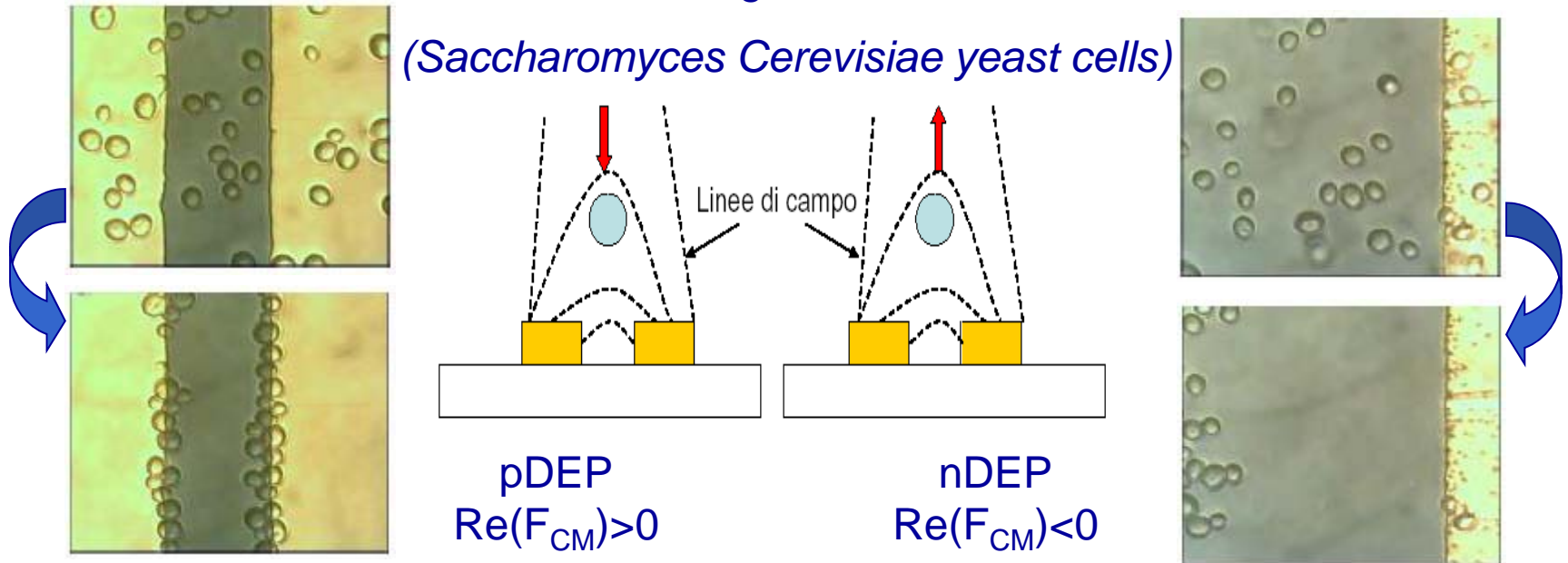
- Time-averaged dielectrophoretic force

$$\begin{aligned} \langle \bar{F}(\bar{r}) \rangle &= 2\pi\epsilon_m R^3 \left[\frac{1}{2} \text{Re}(F_{CM}) \nabla (E_{x0}^2 + E_{y0}^2 + E_{z0}^2) + \text{Im}(F_{CM}) (E_{x0}^2 \nabla \varphi_x + E_{y0}^2 \nabla \varphi_y + E_{z0}^2 \nabla \varphi_z) \right] = \\ &= 2\pi\epsilon_m R^3 \left[\text{Re}(F_{CM}) \nabla E_{rms}^2 + \text{Im}(F_{CM}) (E_{x0}^2 \nabla \varphi_x + E_{y0}^2 \nabla \varphi_y + E_{z0}^2 \nabla \varphi_z) \right] \end{aligned}$$

➔ $\langle \bar{F}_{DEP}(\bar{r}) \rangle = 2\pi\epsilon_m R^3 \text{Re}(F_{CM}) \nabla E_{rms}^2$

Standing wave DEP

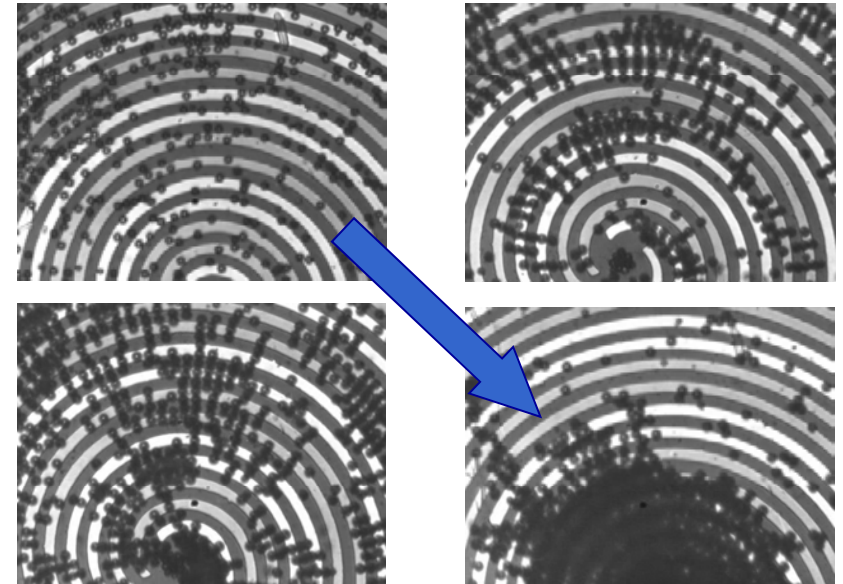
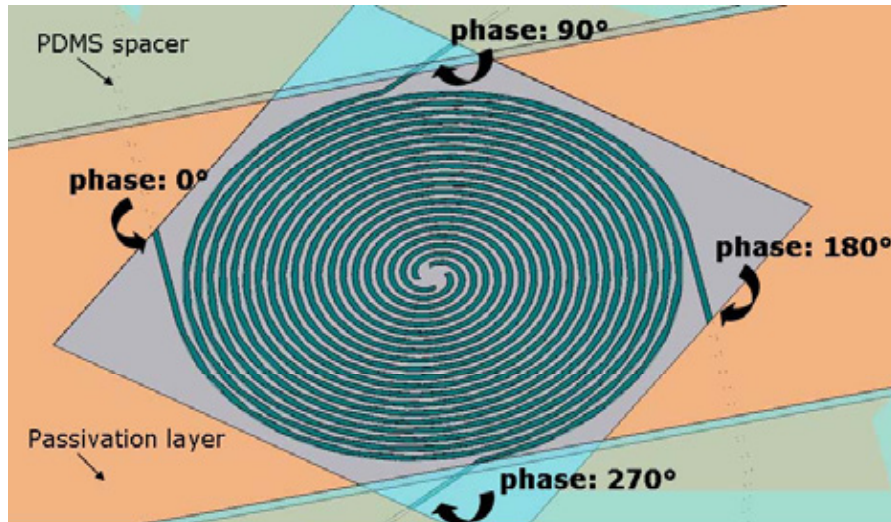
(Saccharomyces Cerevisiae yeast cells)



➔
$$\langle \overline{F}_{TWD}(\overline{r}) \rangle = 2\pi\epsilon_m R^3 \text{Im}(F_{CM}) (E_{x0}^2 \nabla \varphi_x + E_{y0}^2 \nabla \varphi_y + E_{z0}^2 \nabla \varphi_z)$$

Travelling wave DEP

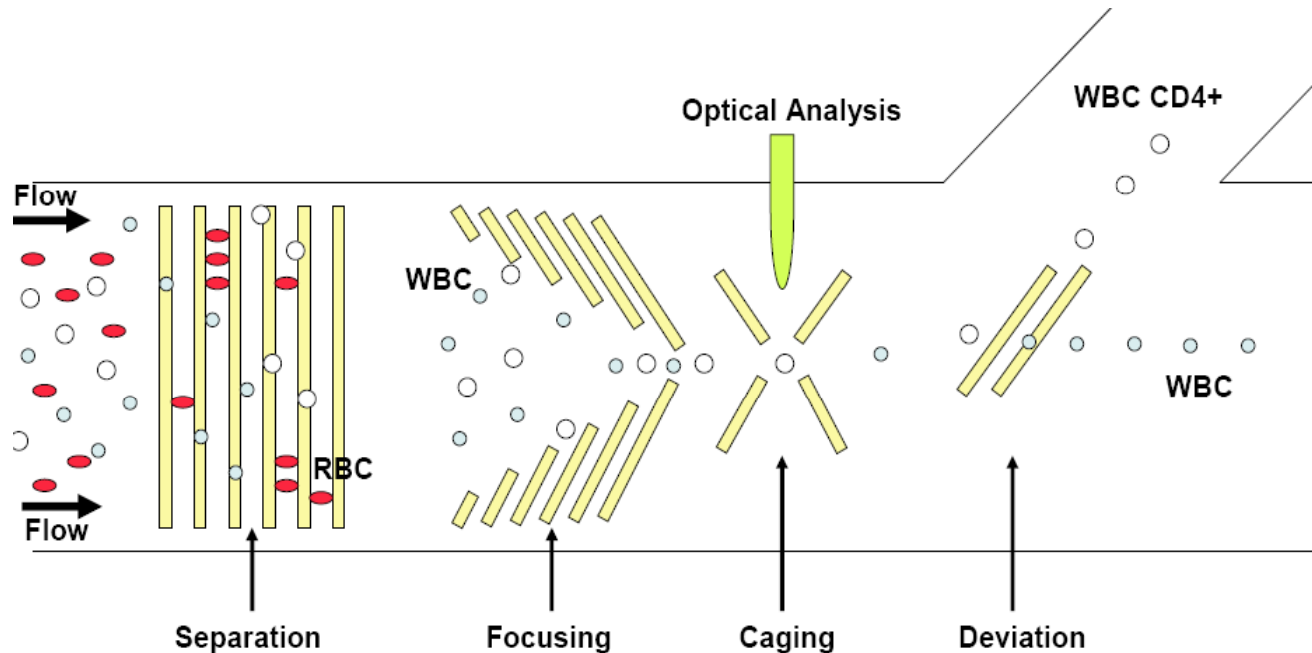
(polystyrene beads, 10 μm in diameter)



The dielectrophoretic modular platform



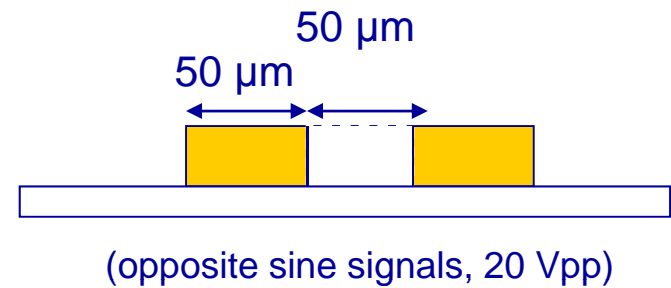
- The dielectrophoretic platform that has been developed is composed of several functional units, organized in a first characterization module and in a series of manipulation stages that can be rearranged on a single chip, depending on the target application (ex: HIV infection level monitoring).



- Numerical and parametrical modelling has been performed to simulate the electric field distribution and to quantify the consequent pico-Newton DEP forces acting at the microscale, in order to optimize the geometry of each functional module.

How to determine the real part of the Clausius-Mosotti factor:

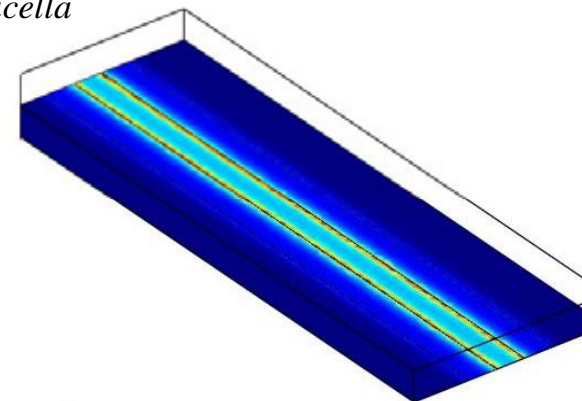
- Measurement of the traslational velocity in a double bar electrode array
- Relation of the real component of F_{CM} with cell velocity of attraction or repulsion (pDEP or nDEP, respectively)



$$\bar{F}_{DEP} = 2\pi\epsilon_m r^3 \text{Re}(F_{CM}) \nabla E_{rms}^2 = 6\pi\eta r U_{particella}$$

$$\text{Re}(F_{CM}) = \frac{3\eta U_{particella}}{\epsilon_m r^2 \nabla E_{rms}^2}$$

Campo Elettrico [V/m]



Max: 6.308e5

$\times 10^5$

6

5

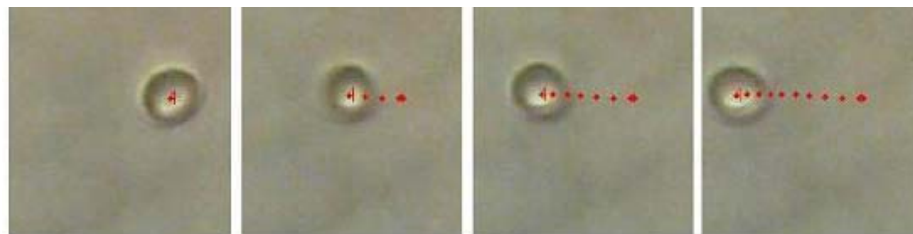
4

3

2

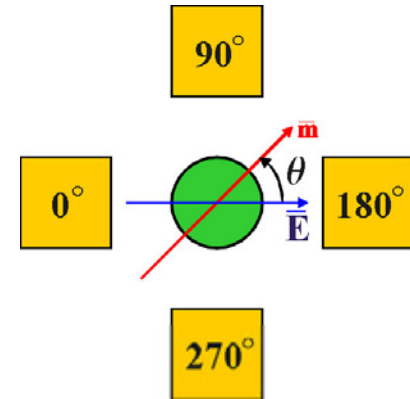
1

Min: 0.259



How to determine the imaginary part of the Clausius-Mosotti factor:

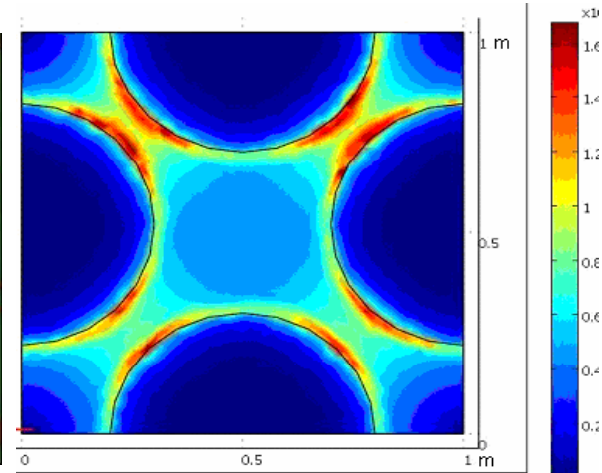
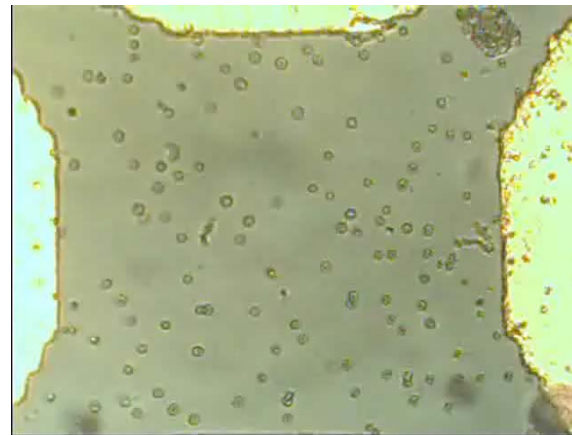
- Measurement of the rotational velocity of cells in the quadrupole configuration
- Relation between the imaginary component of F_{CM} and the rotational velocity of cells



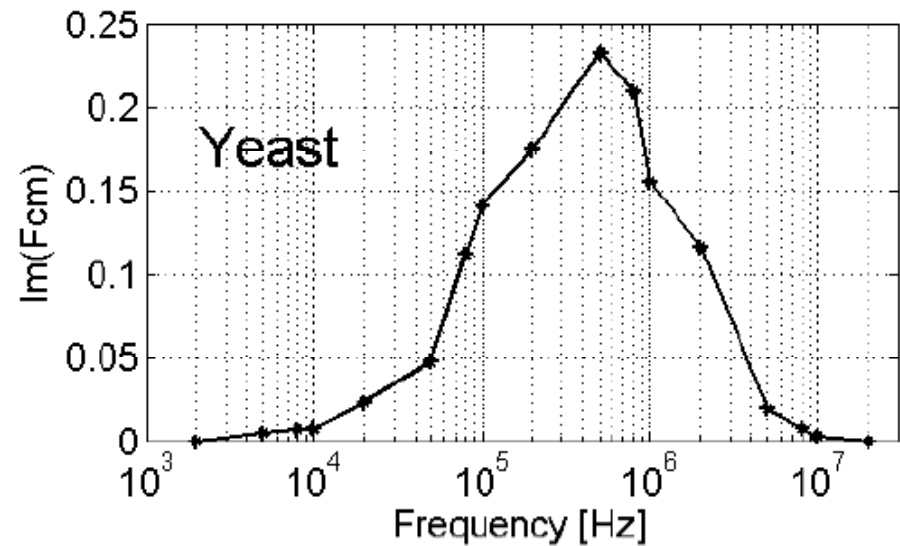
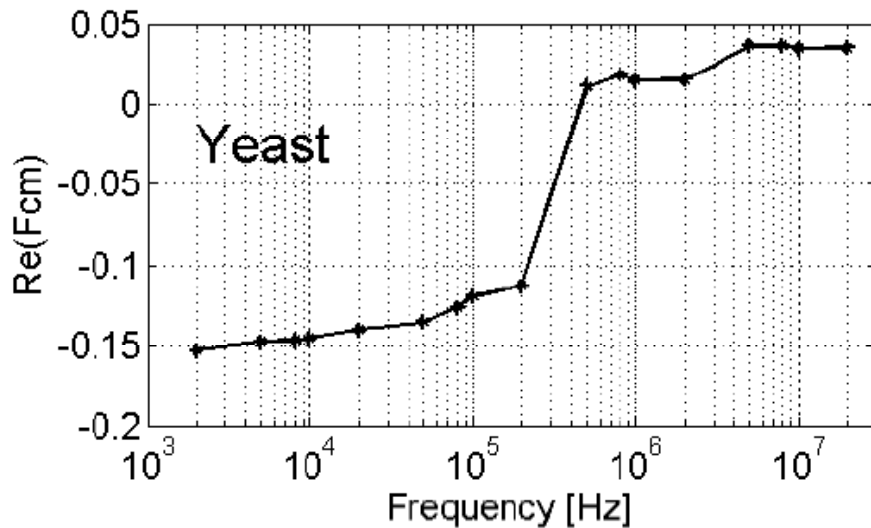
(sine signals in quadrature, 20 Vpp)

$$\Omega(f) = \frac{-4\pi\epsilon_m r^3 \text{Im}(F_{CM}) E_0^2}{6\eta V} = -\frac{\epsilon_m E_0^2}{2\eta} \text{Im}(F_{CM})$$

$$\text{Im}(F_{CM}) = -\frac{\Omega(f) \cdot 2\eta}{\epsilon_m E_0^2}$$



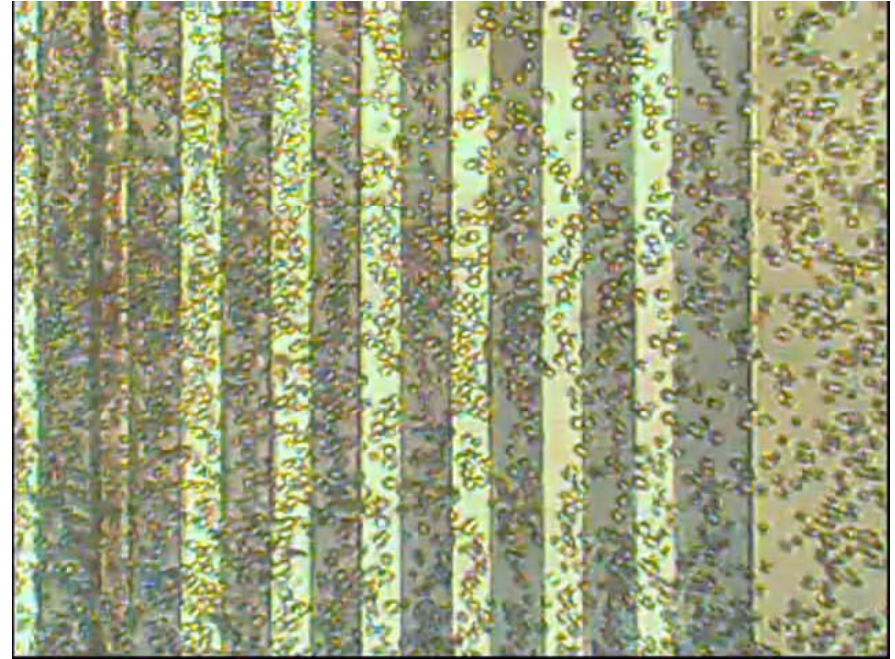
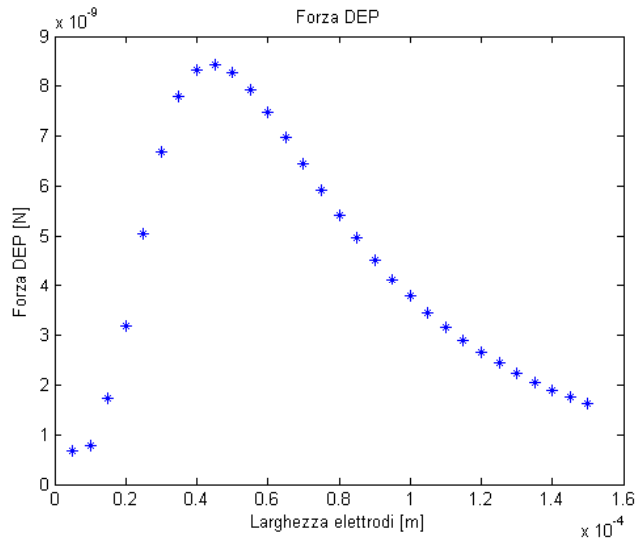
Real and imaginary component of the Clausius Mosotti factor as a function of the frequency of the applied electric field - *Saccharomyces Cerevisiae* yeast cells in a suspension with conductivity $\sigma_m = 435 \mu\text{S/cm}$



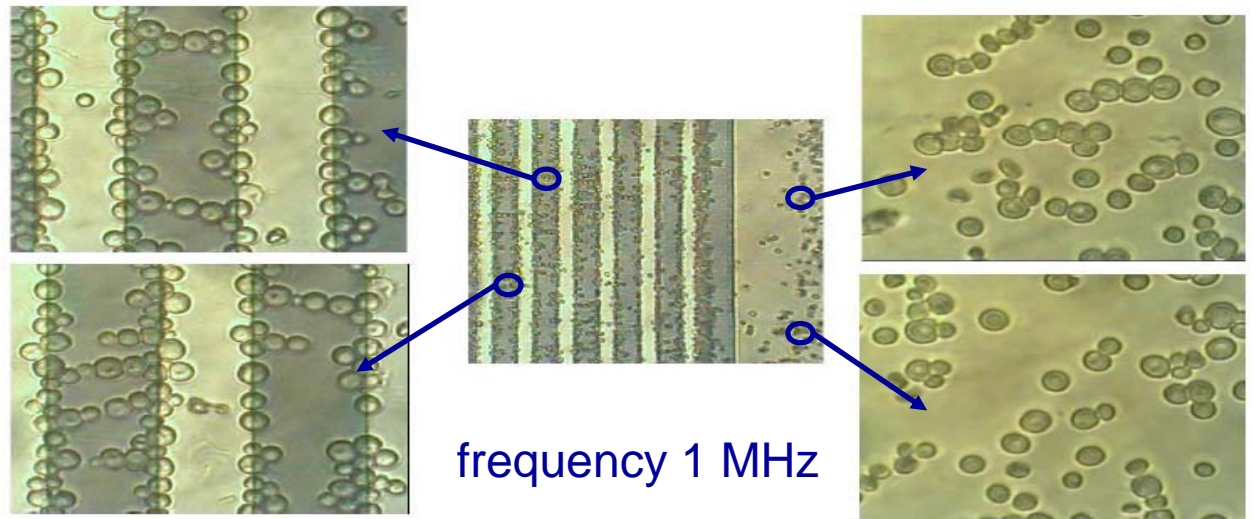
Multi-bar array filter for cell separation



Parametrical modelling
maximizing the DEP force



Separation of
Saccharomyces
Cerevisiae yeast cells
and sheep Red Blood
Cells (RBC)

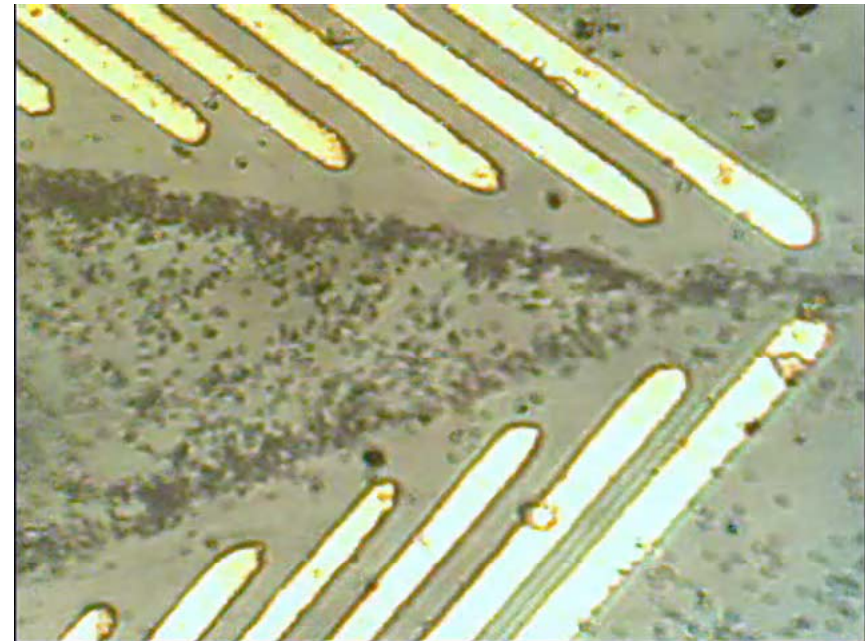
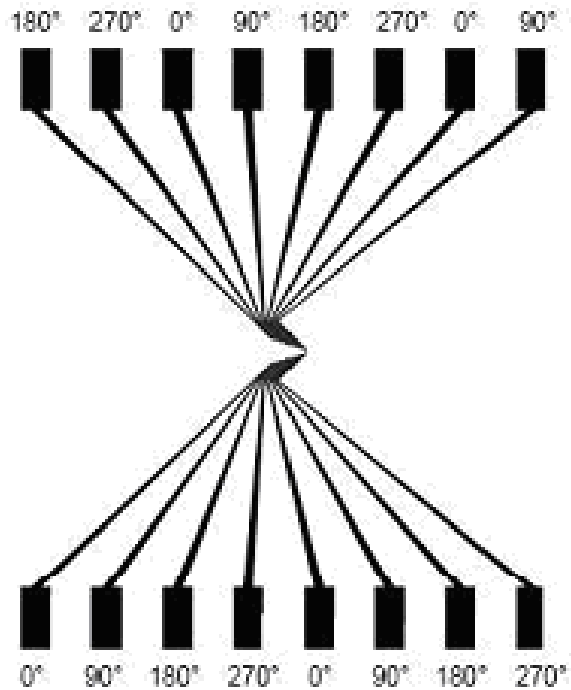
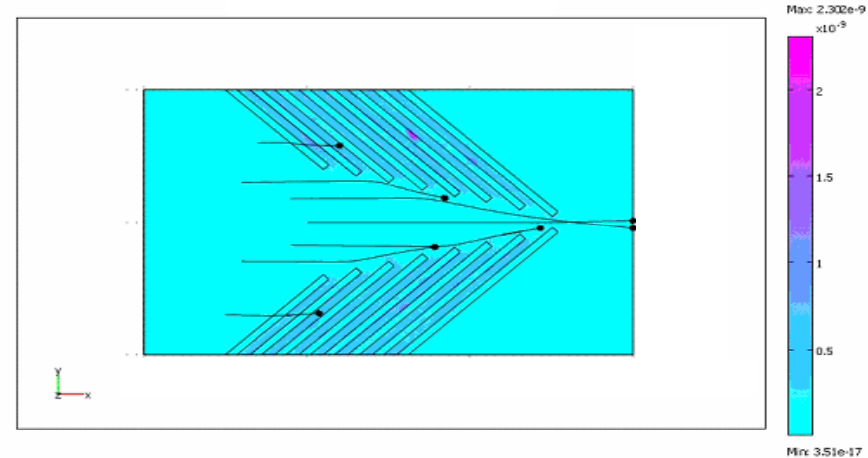


frequency 1 MHz

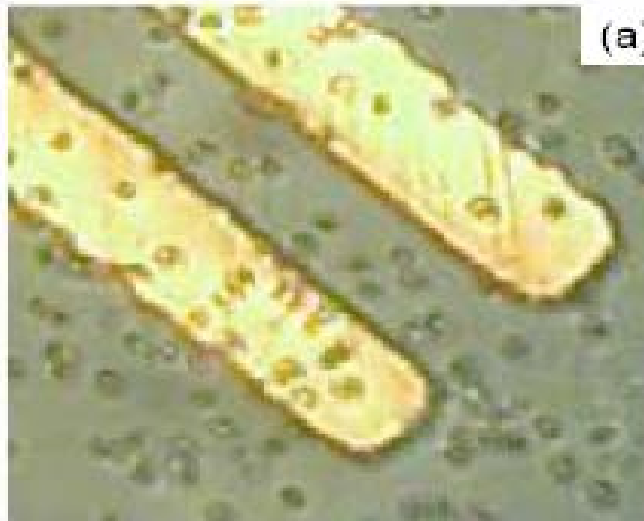
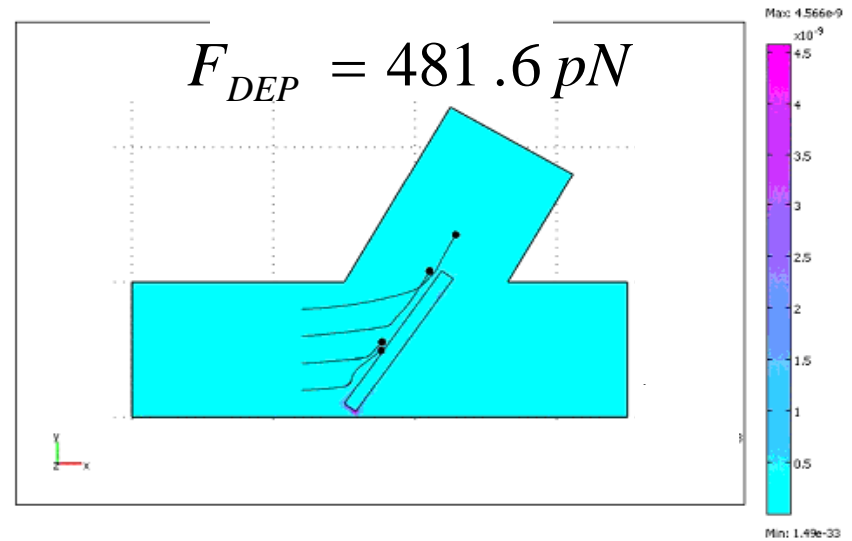
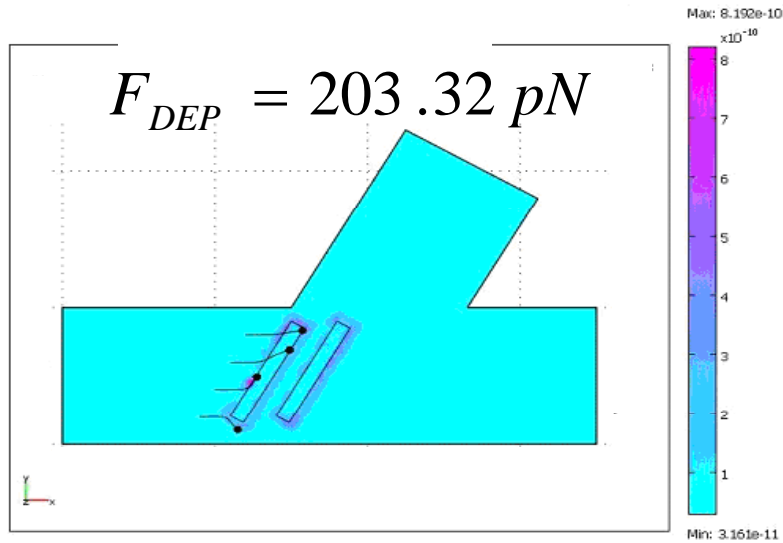
Fishbone-like module for cells focusing



Focusing module:
Saccharomyces Cerevisiae
yeast cells suspension,
conductivity $435 \mu\text{S}/\text{cm}$ and
cell concentration $1.8 \cdot 10^6$
cells/ml



frequency 100 kHz

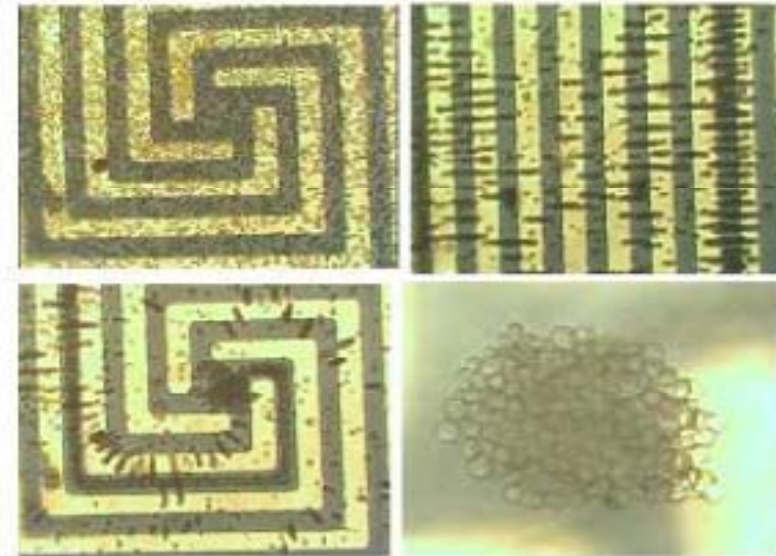
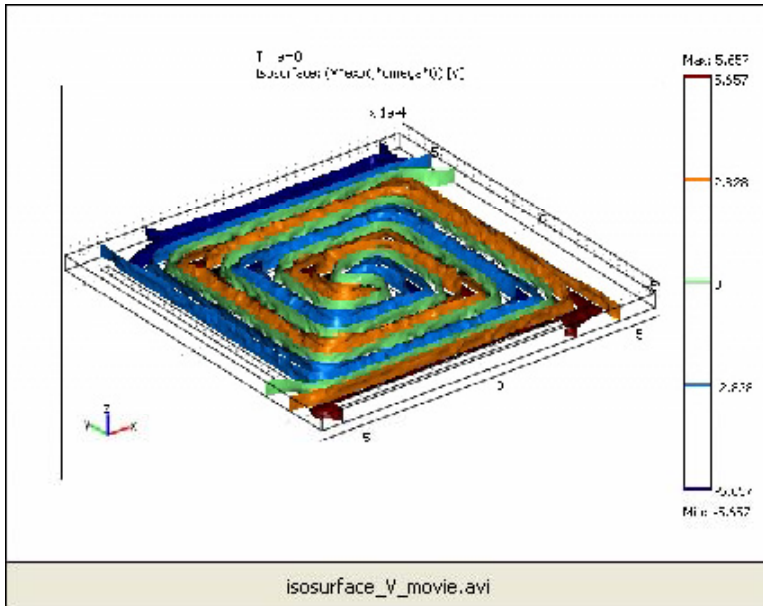


DEP off



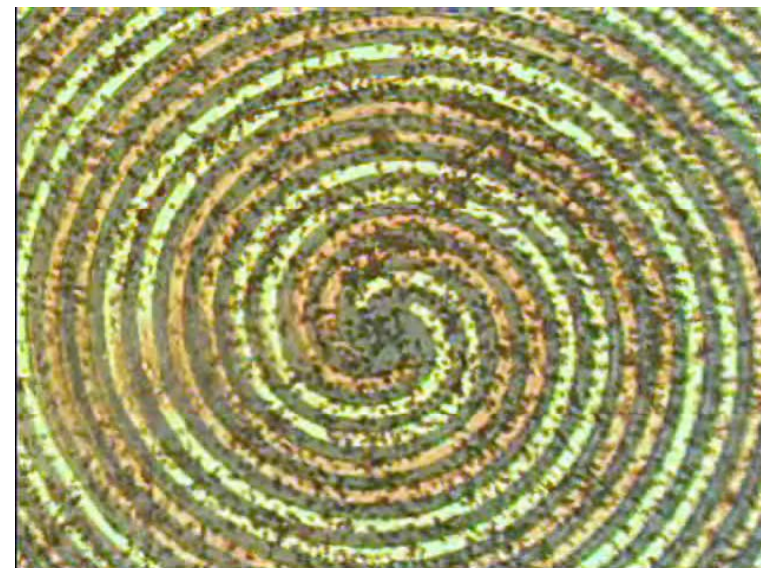
DEP on

frequency 200 kHz



Saccharomyces Cerevisiae yeast cells are concentrated at the center of the spiral array for inspection and counting: numerical simulation and experimental results.

(frequency 100 kHz)



- The functioning of the electrode configurations in the characterization module and in the series of manipulation stages has been demonstrated with different cells types.
- The experimental results and those from modelling are in close agreement.
- The dielectrophoretic platform represents a complete solution, allowing the dielectric characterization of the cell types of interest and their manipulation in applications in which cell handling and sorting are needed.

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